

Visual Medicine: Part Two – Advanced Topics in Visual Medicine



Soft-Tissue Simulation

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Generations of Medical Simulators



1st Generation Simulator:
Geometry/Anatomy/Navigation

- Shape
- Surface & Volume
- Morphology

2nd Generation Simulator:
Physics/Interaction

- Deformation & Forces
- Physical Properties

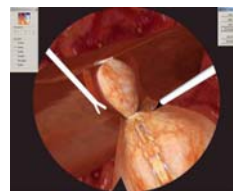
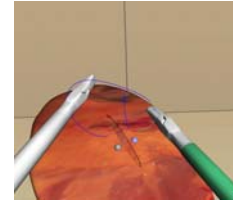
3rd Generation Simulator:
Functional aspects/Physiology

- Pathology
- Function of organs and cells

[Satava 1996, Delinquette 1998]

Classification of training in virtual minimal invasive surgery

- Skill Level
 - Moving instruments
 - Touching locations
- (Basic) Task Level
 - Suturing
 - Clip & Cut a vessel
- Procedure Level
 - Detach and remove gallbladder
- Intervention Level
 - Cholecystectomy



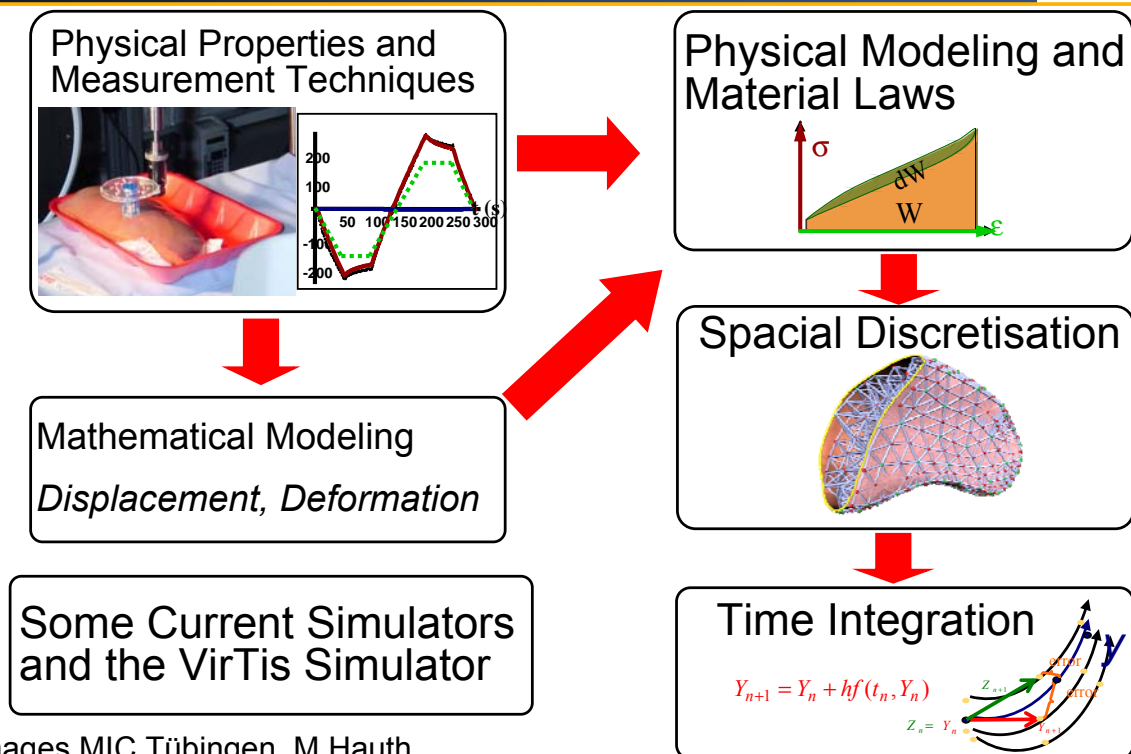
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Soft Tissue Modelling and Simulation

Soft tissue simulation module

- Key technology for 2nd and 3rd generation simulator
- for training beyond task level
- for improving visual realism
- for faithful force feedback
(Non-authentic force-feedback may lead to the adoption of false impressions.)

Accuracy vs. Computation time



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Physical Properties and Measurement Techniques

Soft Tissue deformation is:

1. **elastic:** retreats to rest (spring)
2. **viscous:** damping
but neither uniform nor immediately
3. **plastic:** non-reversible process
tearing, cutting

Blood filled tissue is highly incompressible

Measurements in Biomechanics

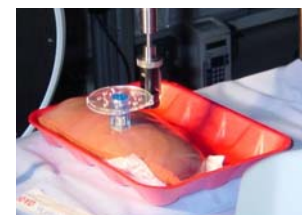
Tissue is Point of Interest in **Biomechanics**

Focusing on skin, vessels, muscles, bone and cells

“Standard” textbook: Fung, *Biomechanics: Mechanical properties of living tissue*

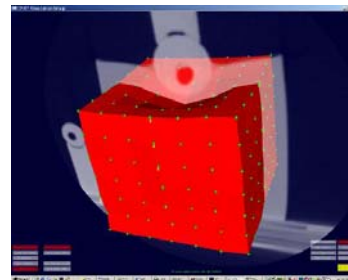
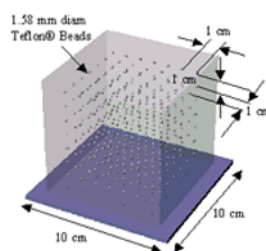
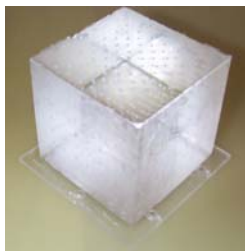
Most work up to mid 90s: **Ex vivo**

Now focussing: **In vivo**



Current Activities

- Enhance database
- Define standard benchmarks:
 - www.truthcube.org,
 - Nava, Valtorta, Mazza (<http://www.zfm.ethz.ch/e/biomechanics/>)

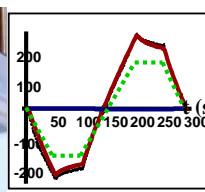
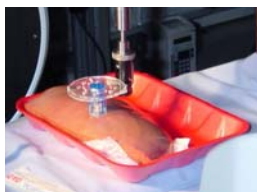


- Comparative measurements [Ottensmeyer 2003]
- Develop better in vivo instruments

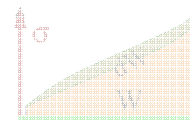
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Mathematical Modeling

Physical Properties and Measurement Techniques



Physical Modeling and Material Laws



Spatial Discretisation



Time Integration

$$Y_{n+1} = Y_n + hf(t_n, Y_n)$$

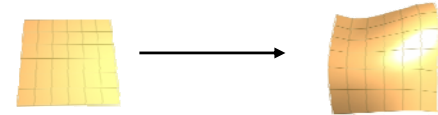
$$Z_n = Y_n + \int_{t_n}^{t_{n+1}} f(t, Y_n) dt$$

Mathematical Modeling
Displacement, Deformation

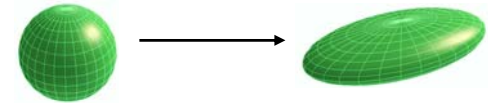
Some Current Simulators and the VirTis Simulator

Mathematical Model

Parametrized Surface: $A: \mathbb{R}^2 \supset K \rightarrow \mathbb{R}^3$

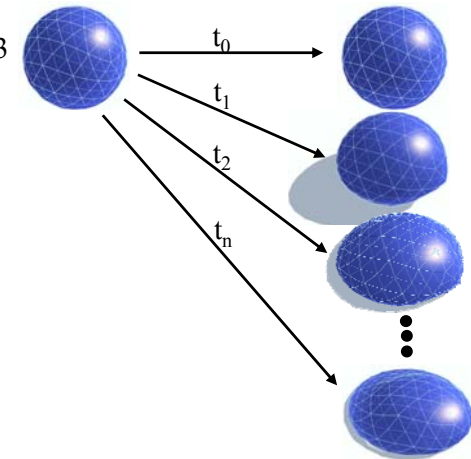


Rigid Body: $S: \mathbb{R}^3 \supset K \rightarrow \mathbb{R}^3$



Deformable Solid: $\phi: \mathbb{R}^3 \supset K \times [0, \infty) \rightarrow \mathbb{R}^3$

Configuration ϕ



Often: initial configuration $K = \phi(\cdot, 0) = \text{id}$

Displacement Field $u := \phi - \text{id}$

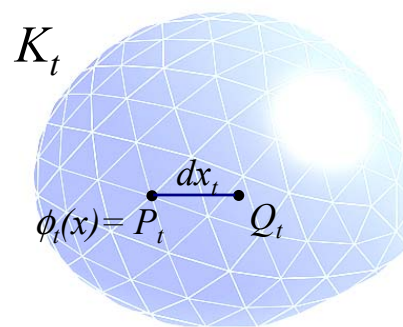
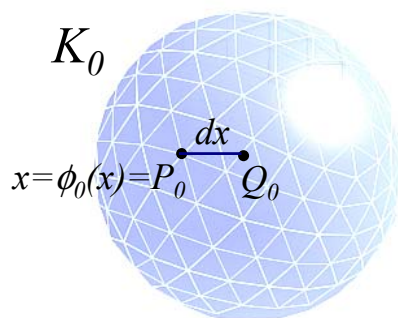
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Soft-Tissue Simulation

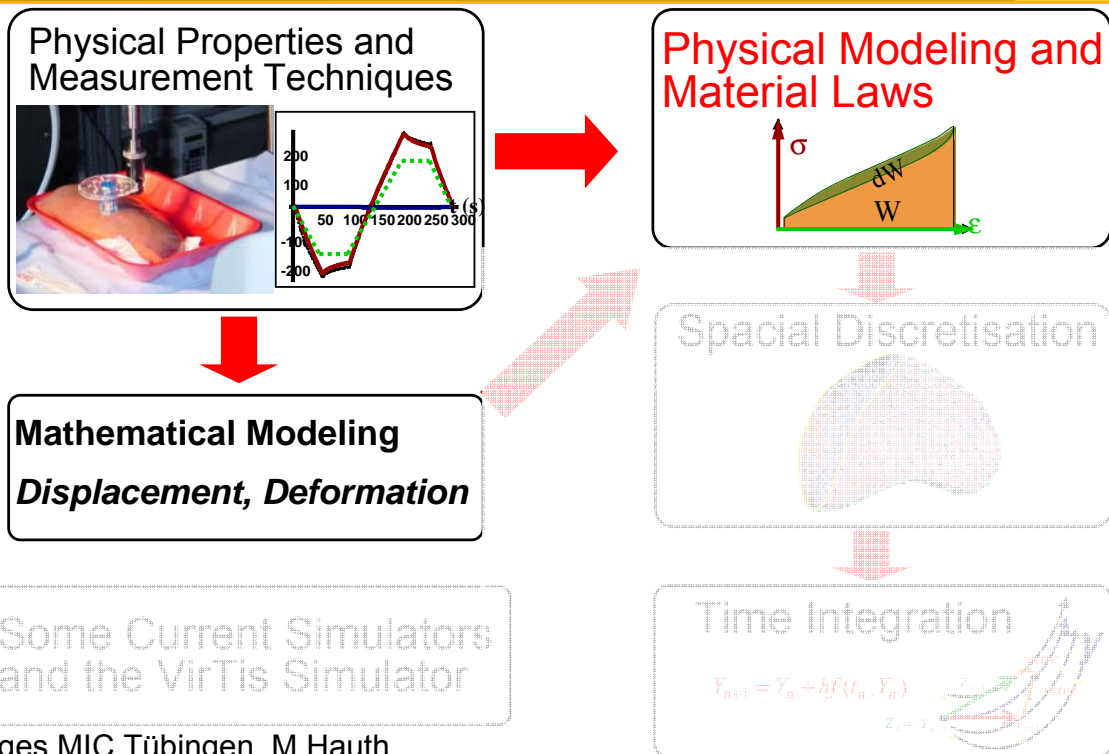
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Measure of Deformation: Strain ε



$$\Rightarrow \|dx_t\|^2 - \|dx\|^2 = \langle \nabla \phi_t dx, \nabla \phi_t dx \rangle - \langle dx, dx \rangle = \langle (\nabla \phi_t^T \nabla \phi_t - \text{id}) dx, dx \rangle$$

Define $\varepsilon := \frac{1}{2}(\nabla \phi_t^T \nabla \phi_t - \text{id}) = \frac{1}{2}(\nabla u_t^T + \nabla u_t + \nabla u_t^T \nabla u_t)$

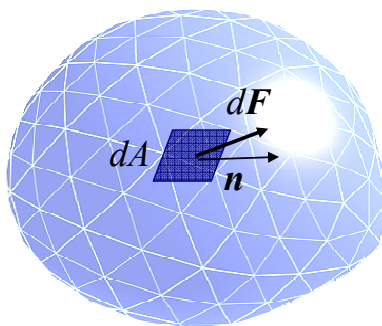


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Material laws

strain tensor ε : geometrical state.

stress tensor σ : internal forces.



$$\frac{dF}{dA} = \sigma \cdot n$$

Assumption: The stress σ is a function of strain (-history).

$$\sigma = \sigma(\varepsilon) = \sigma(\varepsilon(u))$$

Material law.
linear or non-linear

Non-linear for large
strain/displacement
(geometrical non-linearity)

Soft Tissue deformation is:

1. **elastic:** retreats to rest (spring)
2. **viscous:** damping
but neither uniform nor immediately
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tearing, cutting

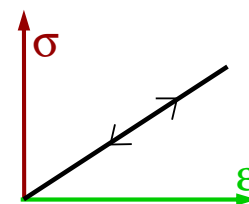
Blood filled tissue is highly incompressible

Material laws

Elastic, isotropic, homogeneous solid:

Hooke's Law

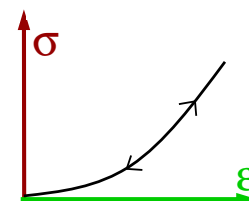
$$\sigma = C\varepsilon$$



Nonlinear elastic solid:

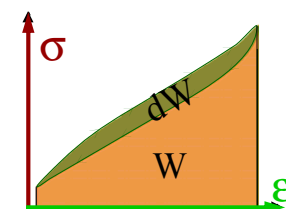
- Mooney-Rivlin
- Neo-Hooke
- Veronda-Westermann

$$\sigma = f(\varepsilon)$$

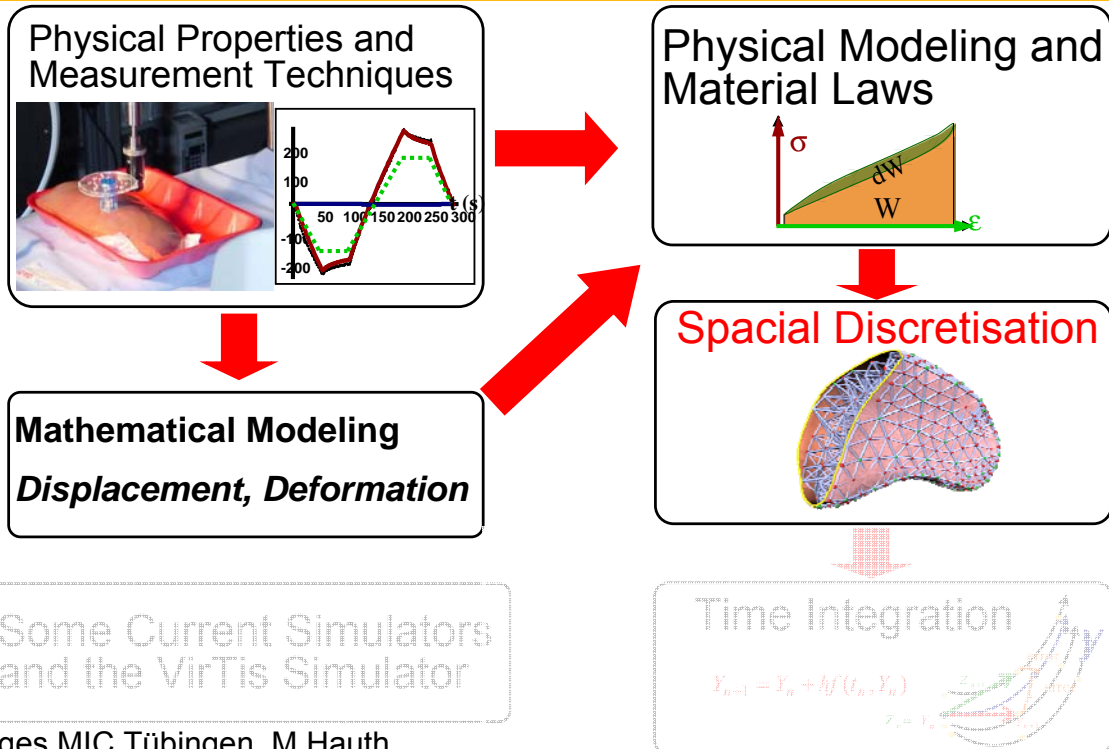


Visco-elastic solid:

$$\sigma(t) = \int_{-\infty}^t R(t-\tau) \dot{\varepsilon}(\tau) d\tau$$

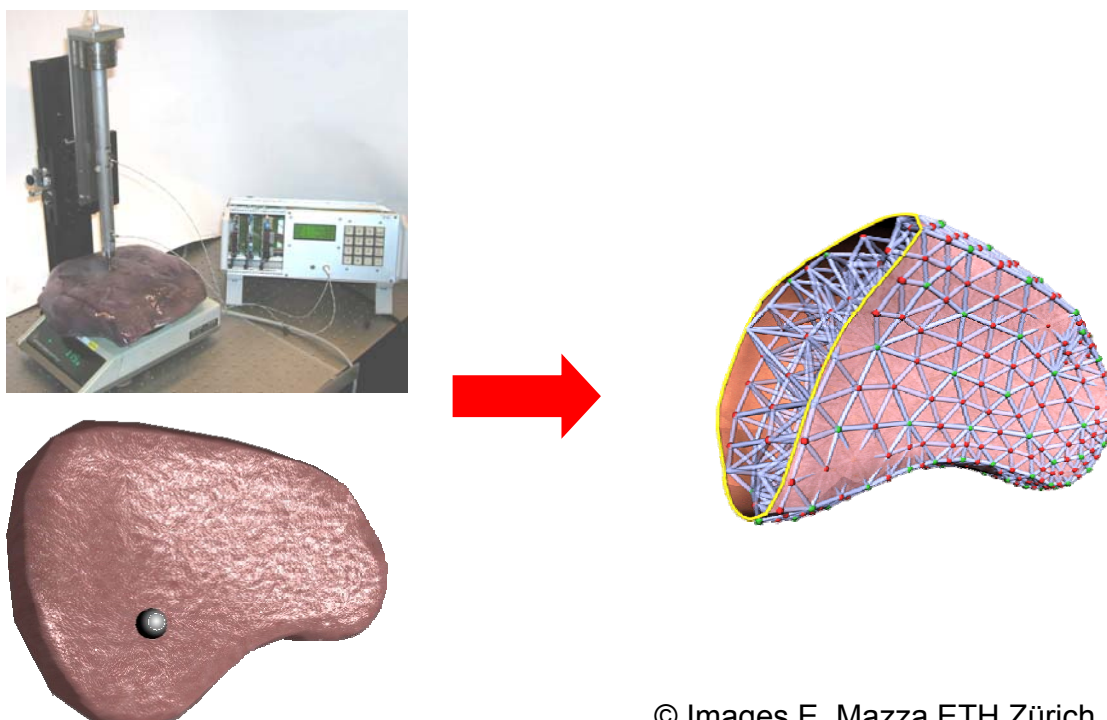


Spatial Discretisation



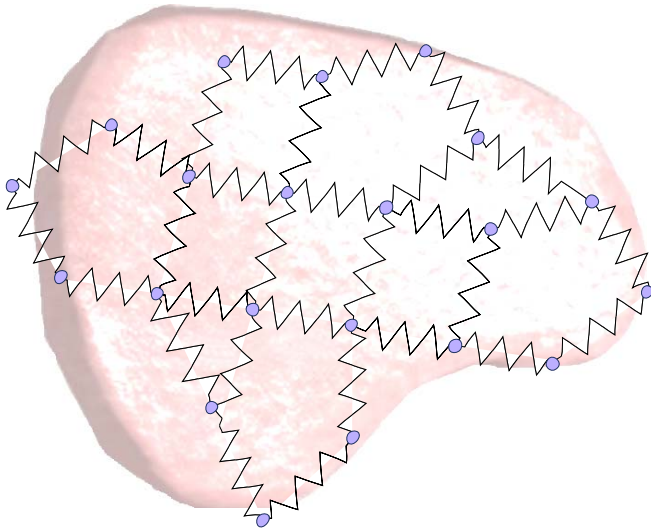
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From Displacements to Simulation



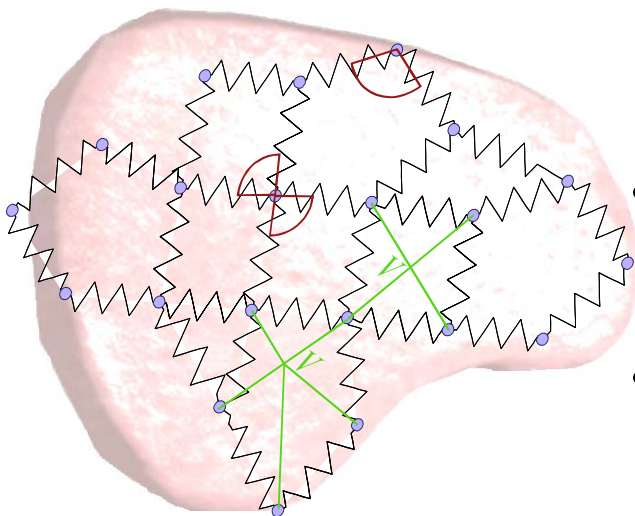
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Mass-Spring/Damper Systems



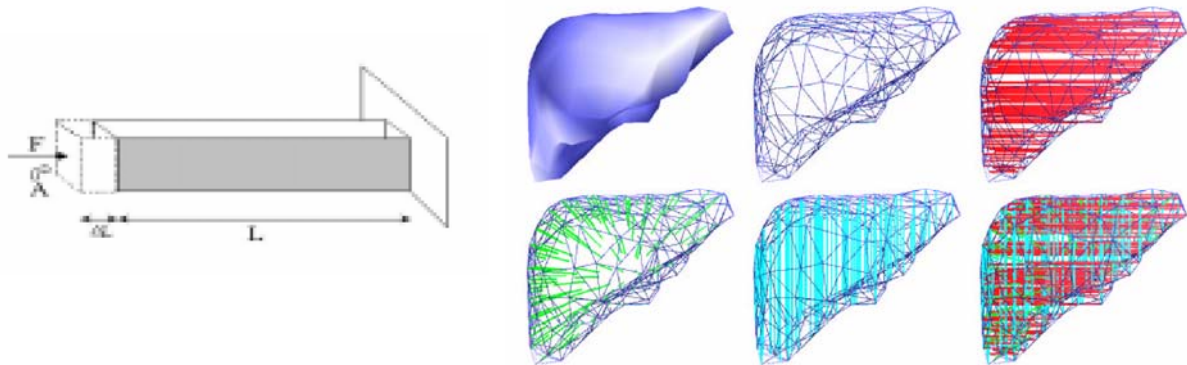
- Arbitrary Topology
- Very difficult to fit to physical data (impossible?)
- Forces defined on edges (pairs)
- Can be over- or underdetermined

Generalized Particle System



- Additional forces to fix shortcomings: **Shear springs**, Bend springs
 - Additional non-spring forces, like **volume preservation**
- **Generalized Particle System**
(Forces between particles)

- Physical simulation of a Long Bar filled with an incompressible fluid.
- Object decomposed into bar elements



[Balaniuk et al. 2000, 2001, 2002; Laugier et al. 2002]

Images taken from Balaniuk and Laugier

Finite Differences / Finite Element Method

- Toolbox to cast a physical formulation into a simulation
- Sound derivation from continuum mechanics
- Standard method in engineering
- Computationally expensive

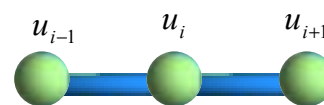
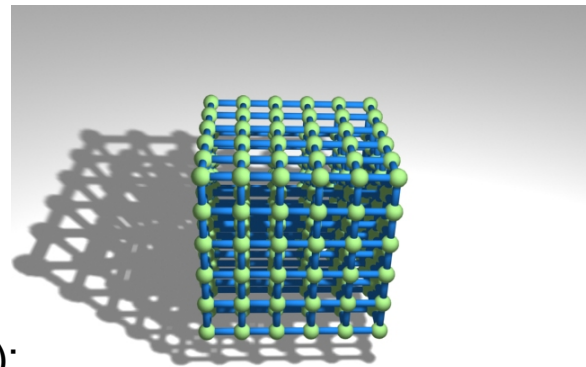
Finite Differences Method (FDM)

$\text{div } \sigma - f = 0$ results in a PDE

- u sampled on *regular* grid
- differential quotients
- ➔ difference quotients (stencils):

$$\frac{\partial u_i}{\partial x} = \frac{u_{i+1} - u_{i-1}}{x_{i+1} - x_{i-1}}$$

$$\frac{\partial^2 u_i}{\partial x^2} = \frac{u_{i+1} - 2u_i - u_{i-1}}{(x_{i+1} - x_{i-1})^2}$$



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Finite Elements (FE)

Approximation with finite d.o.f., with basis φ_i („shape functions“)

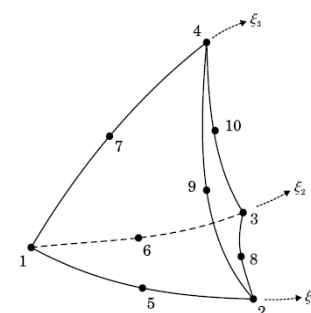
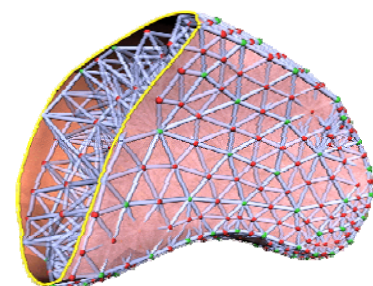
$$u \rightarrow \sum u_i \varphi_i$$

time dependent problem \Rightarrow **ODE**

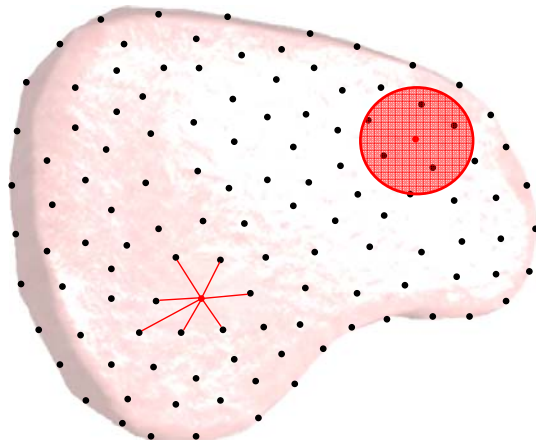
For example: *Linear* trivariate functions :

$$\vec{u}(\vec{\xi}) = \vec{\mu}_0(1 - \xi_1 - \xi_2 - \xi_3) + \vec{\mu}_1\xi_1 + \vec{\mu}_2\xi_2 + \vec{\mu}_3\xi_3$$

or higher order, e.g. quadratic
(more complicate!!)



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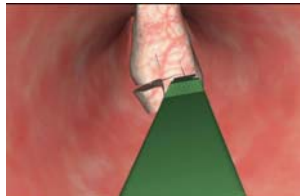


- Arbitrary Topology
- Support zone of each node
- Basis function

$$u \rightarrow \sum u_i \Phi_i$$

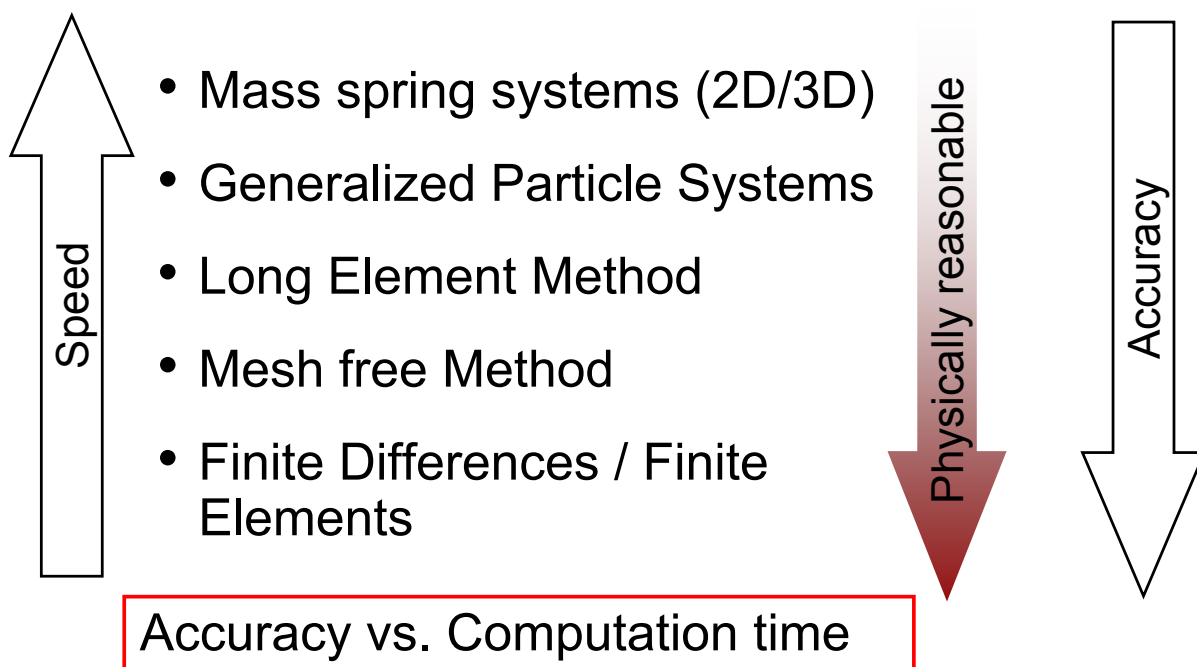
- Very good for tearing, cutting (no remeshing necessary)

- Not real time yet

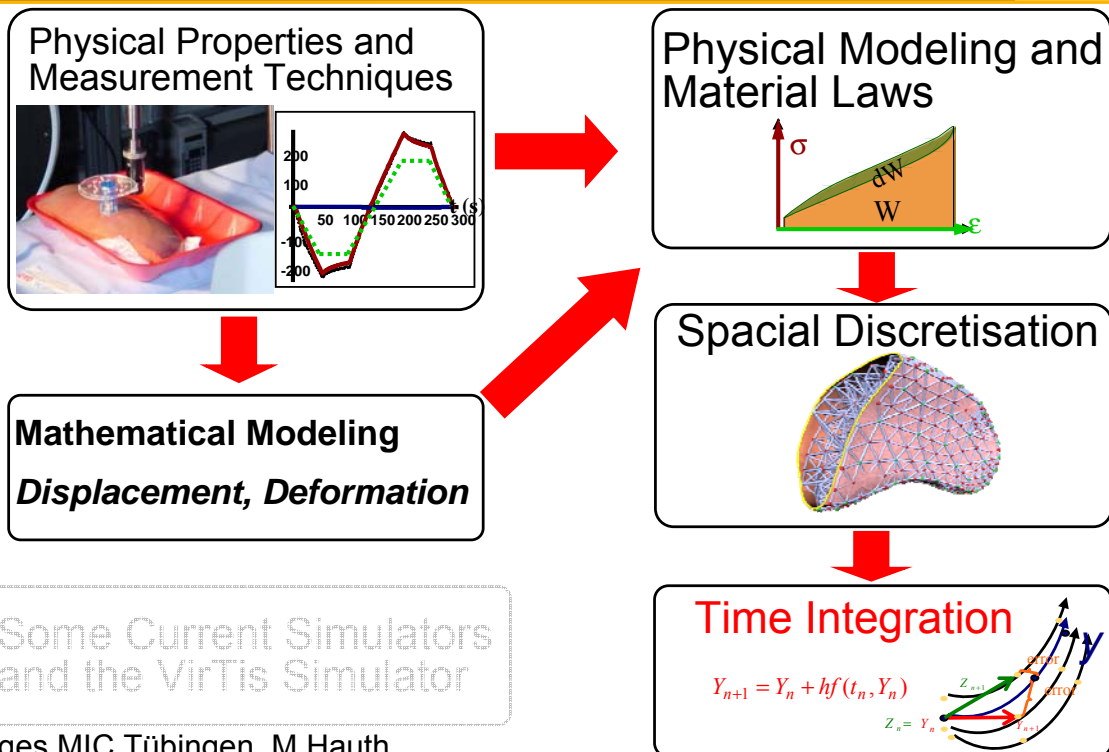


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Methods



Time Integration



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Equations for deformable objects

Equation of equilibrium

$$\delta(E_{elast} + E_{ext}) = 0 \quad \text{div } \sigma - f = 0$$

No inertia and viscosity (dynamical effects)

→ Equation of motion

$$\delta(E_{elast} + E_{kin} + E_{ext}) = 0 \quad \text{div } \sigma + f = \rho \frac{d}{dt} v$$

Discretize: Solve for time steps

Criteria:

- Convergence timestep $\rightarrow 0$
- Accuracy $u_{\text{approx}} - u$
- Stability solution $\rightarrow \infty$
- Efficiency

Numerical Integration

Abstract problem:

$$y' = f(t, y)$$

Goal:

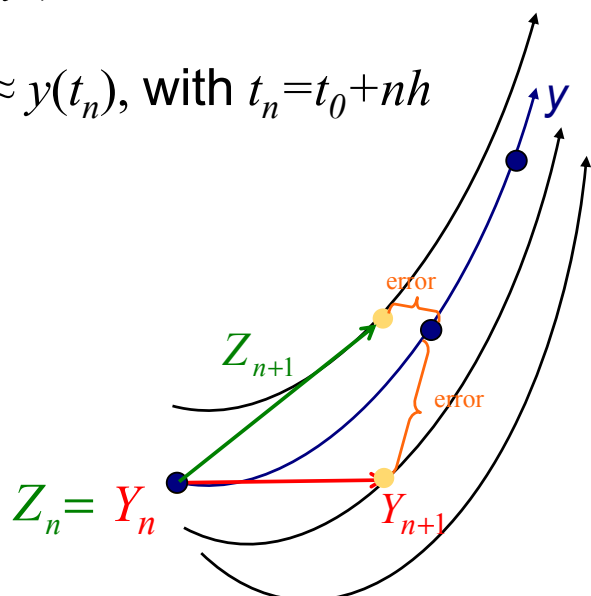
Find approximations $Y_n \approx y(t_n)$, with $t_n = t_0 + nh$

Explicit Euler

$$Y_{n+1} = Y_n + hf(t_n, Y_n)$$

Implicit Euler:

$$Z_{n+1} = Z_n + hf(t_{n+1}, Z_{n+1})$$



Summary: Integration Methods

Implicit methods:

- arbitrary large time steps
- need to solve large (non-)linear systems

Explicit methods:

- Have *strict* time step restrictions
- only need a few function evaluations

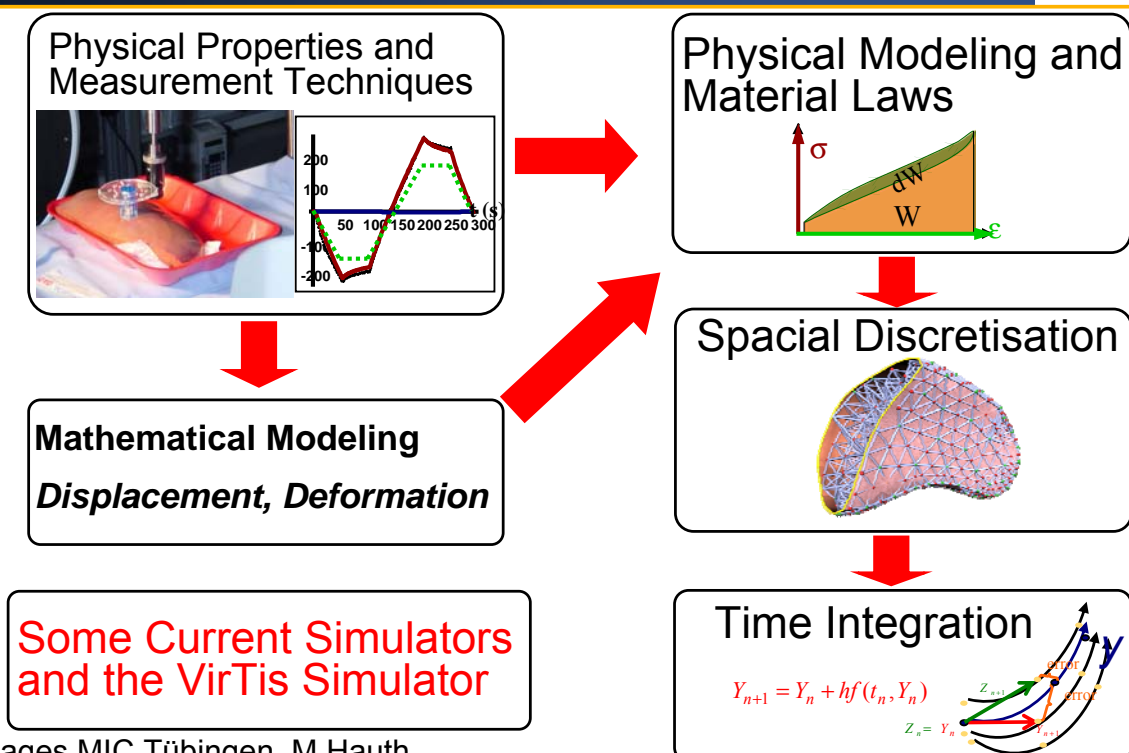
For elastic equations:

- Implicit methods are superior due to large time steps

But they are computationally expensive

- Because the Jacobian changes due to the nonlinearity

Current Simulators



State of the art:

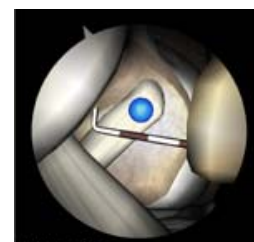
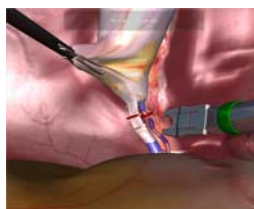
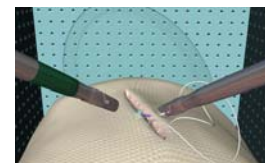
- Mentice, Simsurgery,
- Immersion, Select IT VEST (Kismet), Simbionix, Surgical Science, Xitact
- INRIA Epidaure
- CoMe
- VirTis

Commercial

Research

MIST VR by Mentice / Simsurgery

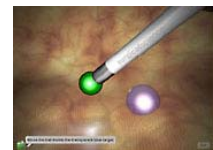
- Focuses on *basic* skills and tasks
- Studies show improved learning
- No force-feedback, thus comparably *cheap*
- Cholecystectomy
- Arthroscopy (shoulder, knee)



- Supposed to use Mass Spring and/or variations of LEM
- Include basic lessons
- Started with cholecystectomy modules
now also cystoscopy, ureteroscopy, ... (in prep. ear-nose-throat surgery)
- Force Feedback, stereoscopic view

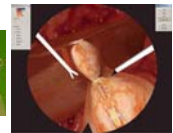
- Immersion Medical (USA)
(www.immersion.com)

LapSim



- Select IT Vest Systems (Germany)
(www.select-it.de)

VS One



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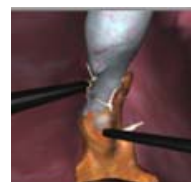
Soft-Tissue Simulation

35/45

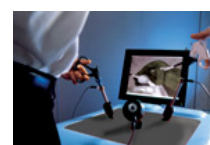
Simbionix (Israel) GI,LAP, URO; PERC Mentor
(www.simbionix.com)



Reachin Technologies (Sweden)
(www.reachin.se)



Surgical Science (Sweden)



XiTact (Switzerland) (www.xitact.com)

LS 500

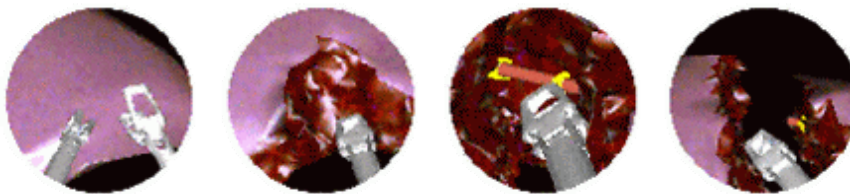
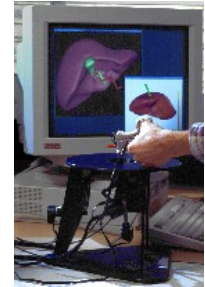
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Soft-Tissue Simulation

36/45

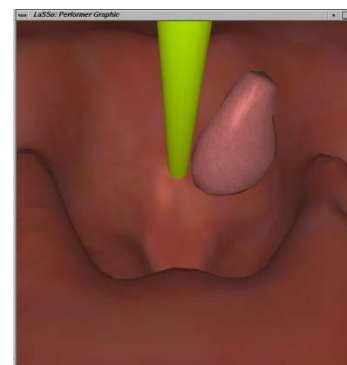
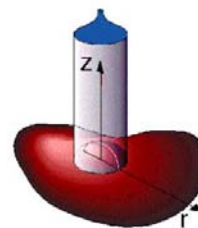
- 1992 - 31.10.2005 , includes tissue modelling as subproject
- New project Asclepios: Medical and Biological Image Analysis
- Finite elements and equivalent tensor mass model
- Anisotropic Hook law
- Force extrapolation for haptic loop



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Lasso / CoMe (co-me.ch)

- Two large Swiss National projects
 - Lasso 1996-2000,
 - CoMe 1st phase 2001-2005, 2nd phase 2006 -)
- Soft tissue part focuses on hysteroscopy
- Includes measurement subproject
- FE, customized mass spring models, mesh free models
- Includes automated texture and pathology generation (e.g. fibroids), and special effects (e.g. bleeding (with CFD))



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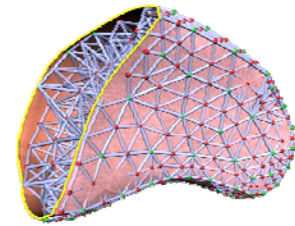
- Cheap basic simulators
- Current commercial simulators lack tissue fidelity
- In comparison to flight simulators, surgery simulators are in the 1930s (flight simulators were accepted in the mid 50s)
- Research simulators are maturing, using almost exclusively the finite element toolbox
- New promising branch: meshless methods

The VirTis Simulator

by WSI/GRIS, Uni Tübingen,

M. Hauth, J. Gross, J. Mezger,
W. Straßer

- Tetrahedral finite elements with linear/quadratic shape functions
- Uses measured data as Prony series, different material laws, e.g. constQ
- Various Implicit or explicit time integration methods
- Haptic feedback with PHANToM



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Demo Movies

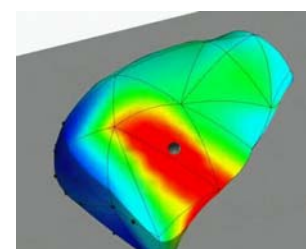
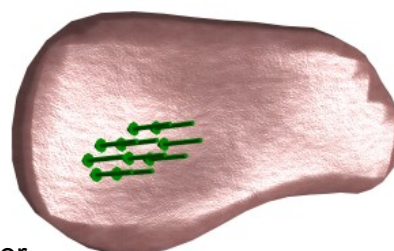
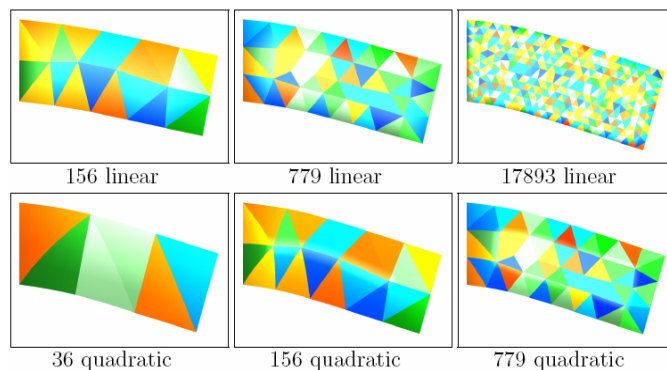
Spring-Model



Visco-elastic-Model



Linear vs quadratic FE



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Summary: The VirTis Simulator



Provides real time finite elements with

- 5 memory parameters
- Real time (full Green strain tensor) :
 - ~ 1000 linear elements
 - ~ 100 quadratic elements } Athlon 64 3500+ (32 bit mode)
- Verification with gold standard (ABAQUS)

Theorie and Applications

**Ph.D. Thesis Michael Hauth, Johannes Mezger
WSI/GRIS, university of Tübingen**

Directions of further work



- Collision
- Tearing, Cutting, Suturing
- Adaptive Subdivision/Coarsening
- Hybrid models (FEM - mesh free)
- Numerical Methods (FEM, time integrators)
- Evaluation of haptic perception
- Parallelization
- ...

Thank you
for your attention